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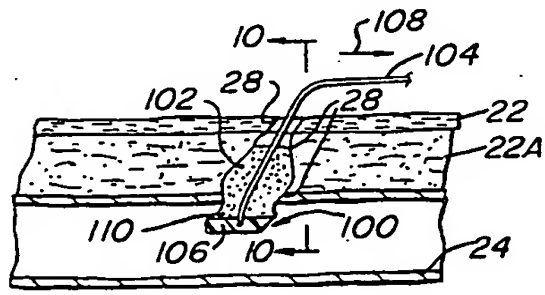
itle: DEVICE FOR SEALING PERCUTANEOUS PUNCTURE IN A VESSEL



bstract

A device (100, 200) and method for sealing a puncture or incision (28) formed percutaneously in tissue separating two inportions of the body of a living being, e.g., a puncture or incision in an artery (24), in the gall bladder, in the liver, in the etc. The device comprises plug means having a holding portion (106) which is adapted to engage portions of the tissue adja- ... opposite an incision to hold the plug means in place and a sealing portion (107) formed of an expandable material which

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DEVICE FOR SEALING PERCUTANEOUS PUNCTURE IN A VESSEL

Field of the Invention

This invention relates generally to medical devices and more particularly to devices for sealing percutaneously formed punctures or incisions.

Background Art

As will be appreciated by those skilled in the art various surgical procedures are now being carried out intravascularly or intralumenally. For example in the treatment of vascular disease, such as atherosclerosis, it is a common practice to invade the artery to insert an instrument, e.g., a balloon or other type of catheter to carry out the procedure within the artery. Such procedures usually involve the percutaneous puncture of the artery so that an introducer sheath can be inserted into the artery and thereafter the instrument, e.g., catheter, itself can be inserted through the sheath to the operative position within the artery. Such procedures unavoidably present the problem of stopping the bleeding at the percutaneous puncture after the procedure has been completed and after the instrument (and any introducer sheaths used therewith) have been removed. At present such bleeding is stopped by the application of direct digital pressure over the puncture site by a trained physician or other suitably trained medical personnel. Such direct pressure has to be applied for a sufficiently long time for hemostasis to occur so that the opening is effectively closed against further bleeding. In the case of punctures into femoral or superficial femoral arteries the pressure may have to be applied for as long as forty-five minutes for hemostasis to occur. Not only is this direct digital pressure application procedure wasteful of time by highly skilled medical professionals, the procedure results in a substantial reduction, if not virtual arrest, of the flow of blood through the vessel. Since thrombosis is one of the major calamities that can occur in the immediate post operative period, any reduction in blood flow, such as caused by the application of digital pressure, is undesirable.

Applicator devices have been disclosed in the patent iterature for inserting an absorbent plug or member into the igina. Such devices basically comprises a tubular element lapted to be inserted into the vagina and having a plug of)sorbent material located therein. The device also includes a .unger to push the plug out of the tubular element into the igina. The plug also includes a thread or string attached to : to enable the plug to be retrieved from the vagina. Examples : such devices are shown in United States Patents Nos. 191,736 (Roberson) and 1,794,221 (Washburn et al.).

While such devices are suitable for their intended irposes, there is no suggestion of their use, nor are they :itable for insertion into an opening in the wall of a blood :ssel or other bodily lumen or duct to seal that opening.

The patent literature also includes devices for closing : opening in a blood vessel using sutures, see United States tent No. 4,587,909 (Gillis). Other means and techniques for osing a wound are disclosed in United States Patent No. 606,337 (Zimmermann et al.).

None of the prior art teaches the use of simple means r effecting the closure of an opening, e.g., puncture, in the ll of a blood vessel, duct or lumen, by plugging the opening d without requiring sutures or the application of digital essure.

A need also exists for devices and methods of sealing rcutaneously formed punctures or incisions in other body ssues such as in the gall bladder, the liver, the heart, the ng, etc.

OBJECTS OF THE INVENTION

Accordingly, it is a general object of the instant vention to provide a device and methods of use which overcome e disadvantages of the prior art.

It is a further object of the invention to provide a vice and methods of use that is effective for closing off a ncture or other opening in a blood vessel, duct or lumen

vithout the need for the application of digital pressure thereto and without resulting in any substantial reduction of blood flow :hrough the vessel.

It is still a further object of the instant invention :o provide an instrument which is simple in construction and vhose method of use entails the ready insertion into a blood vessel, duct or lumen to position a closure therein for iemostatically sealing the puncture and without substantially)locking the flow of fluid through the vessel, duct or lumen.

It is yet a further object of the invention to provide i device and method of use for sealing percutaneously formed)unctures or incisions in tissue separating two portions of the)ody of a living being from the flow of a body fluid :herebetween.

SUMMARY OF THE INVENTION

These and other objects of the instant invention are ichieved by providing a device and method for sealing a puncture)r incision formed percutaneously in tissue separating two nternal portions of the body of a living being, such as)unctures or incisions in blood vessels, ducts or lumens, gall)ladders, livers, hearts, etc. The device comprises a tubular)ody having an outlet at the distal end thereof and which is dapted to be inserted through the puncture or incision to expel . closure therefrom. The closure comprises a first holding)ortion adapted to engage portions of the tissue adjacent the)uncture or incision to hold the closure in place and a second ealing portion formed of an expandable material (e.g., a foam) hich is adapted to extend through the puncture or incision and hich expands automatically in response to the ambient urroundings when in the body of a living being to engage the issue contiguous with the puncture or incision to seal it from he flow of a body fluid therethrough between the two body ortions.

BRIEF DESCRIPTION OF THE DRAWING

Fig. 1 is a side elevational view partially in section howing a portion of one device constructed in accordance with his invention about to be inserted into a conventional sheath xtending through a percutaneous puncture into an artery;

Fig. 2 is a side elevational view of the device 20 in lace in the sheath;

Fig. 3 is a side elevational view of the device 20 uring the expulsion of its puncture sealing closure into the rtery;

Fig. 4 is a side elevational view of the artery showing he sealing closure in place to close off the percutaneous uncture;

Fig. 5 is a reduced plan view of the device 20 of the ubject invention;

Fig. 6 is a side elevational view of the device shown n Fig. 1 but including an alternative embodiment of the losure;

Fig. 7 is a sectional view taken along line 7-7 of Fig. ;

Fig. 8 is a side elevational view of the embodiment of ıe device shown in Fig. 6 during the expulsion of its puncture ealing closure into an artery;

Fig. 9 is a side elevational view similar to that of ig. 8 but showing the puncture sealing device in place within ıe puncture in the artery;

Fig. 10 is a sectional view taken along line 10-10 of ig. 9.

Fig. 11 is a sectional view through the body of the ing showing the sealing of a percutaneous incision or puncture ı the gall bladder and liver; and

Fig. 12 is a sectional view through the body of the ing showing the sealing of a wound in the lung and heart.

Detailed Description of the Preferred Embodiment

Referring now in greater detail to the various figures of the drawing wherein like reference characters refer to like parts, there is shown generally at 20 in Fig. 1 an instrument for effecting the closure of a puncture or other opening in a blood vessel, duct or lumen in a living being. The device 20 thus has particular utility when used in connection with intravascular procedures, such as angiographic dye injection, balloon angioplasty and other types of recanalization of therosclerotic arteries, in-situ valvulectomy, etc. However, it should be appreciated that the device 20 can be used to hemostatically close a puncture or other opening in othe types of duct or lumens within the body. Thus, it is to be understood that while the description of the invention as contained herein is directed to closing off percutaneous punctures in arteries, the device 20 has much more wide-spread applications.

Before describing the instrument 20 itself a brief description of a typical, conventional, intravascular surgical procedure, e.g., catheter instrumentation of an artery, utilizing a percutaneous incision or puncture will be given to best appreciate the features of the device 20. In such a procedure a cannula of an instrument, such as an angiographic needle (not shown), is inserted percutaneously through the skin into the artery, such as the femoral artery 24 at the situs for the instrument's insertion. The needle cannula is held in place and the flexible end of a mini-guidewire (not shown) is then passed through the cannula into the artery to the desired depth (i.e., longitudinal position therealong). Once the mini-guidewire is in place the needle cannula is removed leaving the guidewire in place. A conventional introducer sheath 26 and a arterial dilator (not shown) are then passed over the guidewire through the puncture 28 and into the artery 24. The guidewire and then the dilator are removed leaving the sheath 26 in place. The catheter (not shown) or other intravascular instrument (not shown) is then inserted through the introducer sheath 26 and threaded down the artery to the desired

ntravascular location, e.g., the situs of an atherosclerotic cclusion. Once the intravascular procedure (e.g., angioplasty) as been completed the catheter is removed. Thereafter the heath is removed and the surgeon or other trained person pplies digital pressure to the percutaneous puncture until emostasis has occurred.

The device 20 effects the hemostatic closure of a ercutaneous or other type of puncture, incision or opening in n artery or other body duct or lumen without necessitating the pplication of pressure thereto. Thus, once the catheter or ther intravascular instrument has been removed but with the ieath 26 left in place, the device 20 of the subject invention s inserted through the sheath 26 into the artery 24 and perated to expel a closure member 30 (to be described later) ito the artery. The closure is arranged to be drawn back into ie puncture 28 to seal it. The sheath is removed and the losure left in place. Due to its construction the closure is timately absorbed by the surrounding tissue.

As can be seen in Fig. 1 the device 20 basically com- ises a tubular body 32 having an outlet 34 at its distal end, ie heretofore identified closure member 30 having a retraction lament 36 connected thereto, and pusher means 38. The tubular dy is an elongate member preferably constructed of a fficiently small outside diameter, e.g., 8 F (French), and mewhat flexible material, such as polyethylene or polyvinyl- loride, to enable it to be inserted through the introducer eath 26 into the artery 24, with the tubular body's outlet 34 thin the artery distally of the puncture 28.

The closure member 30 is an expandable member which, en contracted or compressed is sufficiently compact to fit thin the interior of the tubular body 30, but when constrained by the tubular body it expands to an enlarged nfiguration (See Figs. 3 and 4) suitable for closing off the ncture 28 in the artery. Thus, closure member 30 is formed a resilient, hemostatic material, which is preferably odegradable, so that it need not be removed after placement.

One particular effective material is a porous hemostatic absorbable gelatin sold by Johnson & Johnson, Inc. under the name Gelfoam.

The pusher means 38 basically comprises an elongated, cylindrical rod-like member, having a distal end 40. The pusher is also formed of a relatively flexible material, such as polyethylene or polyvinylchloride and is disposed within the interior of tubular body 32. The outside diameter of the pusher is slightly less than the inside diameter of the tubular body portion to enable the pusher to be manually moved (slid) down the longitudinal axis of the body portion 28, to push or force the closure 30 out of the outlet 34. Thus the pusher is arranged to be moved from a retracted position, like that shown in Fig. 2 to an extended position like that shown in Fig. 3 herein its distal end 40 is located close to the outlet 34 of the body 32. When the pusher is moved to the extended position its distal end forces the closure member 30 out of the outlet 34.

The heretofore identifed retraction filament 36 constitutes an elongated thread, preferably formed of a long, yet very thin, biodegradable material, such as an absorbable suture, and is fixedly secured to the proximal side 42 of the closure member 30 at the middle thereof. When the closure is in position within the tubular body the thread 36 extends down the length of the tubular body 32 between it and the pusher 38 so that the proximal end of the thread is located outside the device 20.

The thread 36 being long and thin does not interfere with the operation of the pusher expelling the closure member 30 out of outlet 34. Thus, during the expulsion of the closure into the artery the thread 36 slides down the tubular member with the closure. The thread 36 is sufficiently long that a substantial length extends outside of the proximal end of the device 20 even after the closure is in the artery.

In order to effectuate the movement of the pusher from the retracted to the extended position the tubular body includes collar 44 having a flanged projection 46 arranged to be

rasped by the fingers of the user of the device 20. In ddition the proximal end 48 of the pusher 38 includes an nlarged cap 50 arranged to be engaged by the user's thumb. hus, to effect the ejection of the closure member 30 all the ser of the device 20 merely has to do is to grasp the rojection 46 with his/her fingers while applying pressure to he cap 50 with his/her thumb. This action forces the pusher own the tubular body to the extended position.

As can be seen in Figs. 3 and 4, when the closure ember 30 is in its unconstrained state (such as when it is jected into the artery) it assumes a configuration having an nlarged head portion 52 and an anchor portion 54. The head ortion is of generally disk-like shape of relatively large iameter, e.g., 6-9 mm, yet relatively thin, e.g., 1-2 mm. The ead portion includes the rear (proximal) surface 42 and a front listal) surface 56. The anchor portion 54 consists of a small iameter, e.g., 2-3 mm, hub-like projection from the proximal rface 42 at approximately the center thereof. The distal end the retraction thread 36 is fixedly secured to the anchor ortion 54. The resilient nature of the closure enables the nlarged head portion 52 to conform to the surface 58 of the nterior of the artery 24 contiguous with the puncture 28 so nat its proximal surface 42 intimately engages the artery rface 58 while the hub-like anchor portion 54 extends somewhat nto the puncture 28 to hemostatically seal the puncture when ne closure is pulled into place, as will be described reinafter.

Thus, as shown in Fig. 3, after the tubular body 32 of vice 20 has been inserted into the sheath 26 so that its tlet 34 is within the artery, the sheath 26 is withdrawn. The sher is then extended or pushed down the tubular body as scribed heretofore so that its distal end portion 40 forces ne closure 30 out of outlet 34. Once the closure 30 is outside ne confines of the tubular body 32 it expands or enlarges to s disk-shaped configuration. After the closure is pushed out the tubular member by the pusher, the tubular body is itself

withdrawn from the puncture 28 in the artery and moved completely outside the body of the patient. This action leaves the closure 30 within the artery and with the retraction filament extending through the puncture 28 so that a substantial portion of the filament is outside the patient's body. The filament is then pulled by its proximal end to cause the closure to move toward the puncture 28, until its anchor portion 54 is somewhat within the puncture and its engagement surface 42 is in intimate engagement with the interior of the artery wall contiguous with the puncture. This action hemostatically seals the puncture. In order to hold the closure in place the thread 34 is held taut and is secured in position on the patients skin, such as by use of a strip of conventional tape 60. Alternatively, some other gripping means (not shown) can be used to slide down the filament into contact with the skin while together gripping the filament tightly to prevent it from slipping.

By virtue of the fact that the head portion 52 of the closure is thin and conforms to the interior surface of the artery, it does not block off or otherwise impede the flow of blood through the artery.

It should be noted at this juncture that the closure can be of any suitable shape and need not be of the disk-like shape shown herein, so long as once it is puled into position at the situs of the puncture it serves to hemostatically seal that puncture without appreciably blocking the passageway. Moreover, in order to minimize the risks of thrombosis in the artery the front (distal) face 56 of the closure 30, which is exposed to the flow of blood through the artery, may be coated with a non-thrombogenic material. This feature serves to minimize the risk of thrombosis forming in the artery. The thrombogenic material used can comprise a waxy coating, such as coconut oil, on the closure's front surface 56.

As mentioned earlier the closure and its retraction filament are each preferably formed of an absorbable (e.g., biodegradable) material. This feature enables the closure to be

eft in place after hemostatis has occurred since it will be osorbed by the bodily tissues thereafter. Accordingly, the losure does not have to be removed after having served its irpose.

In order to accellerate hemostasis the natural forming ie closures of this invention may include conventional clotting jents, such as tissue throboplastin.

In Fig. 6 there is shown an alternative embodiment of ie closure utilized in a device 20 for sealing a percutaneous incture or incision. The alternative embodiment of the closure s designated by the reference numeral 100 and basically mprises three components, namely, a holding member 106, a iture or filament 104, and a sealing member 102. The holding mber 106 is an elongated body constructed like a toggle and is referably formed of a biodegradable, thermoplastic polymer, ich as polyglactide. This material will degrade within the dy within a short period of time, e.g., approximately 45 days. ie toggle is molded onto the distal end of the filament 104 iich is slightly bulbous to hold the toggle in place thereon. ie filament is also preferably formed of polyglactide (e.g., it .ll degrade within the body in approximately 90 days). The .lament is quite flexible so that the toggle can pivot to irious orientations with respect to it. Disposed promixally hind the toggle 106 is the sealing member 102. That member isically comprises a cylindrical plug preferably formed of a mpressed foam which is highly absorbent and which, when sposed within the body, swells in excess of its compressed ameter, e.g., swells to twice its compressed diameter. The ug is preferably formed of gelatin or collagen foam so that it so degrades quickly within the body, e.g., in approximately n days or so. The filament extends fully through the plug.

The closure 100 is located within the device 20 ljacent the outlet 34 of the tubular portion 32 thereof. In irticular, the foam plug or sealing portion 102 is located mediately adjacent the free end 40 of the plunger 38, with the ggle or holding portion 106 located at the distal end of the

portion 102. The toggle is oriented so that its longitudinal axis is parallel to the longitudinal axis of the device 20. When so disposed the toggle compresses a portion of the distal end of the plug portion. The filament 104 extends backward from the toggle portion through the plug portion and through a central passageway in the plunger 38 to a point outside the device 20. The closure is introduced into the artery, or into a puncture or incision in any body tissue, such as the liver (Fig. 11), gall bladder (Fig. 11), lung (Fig. 12), heart (Fig. 12), etc., until the insertion device's outlet 34 is in the desired position.

In the case of the sealing of an artery, the outlet 34 of the device is positioned so that it is within the artery (See Fig. 8) and just slightly beyond the introducer sleeve 26. This placement is controlled by stops (not shown) on the device 20. The plunger 38 is then operated as described earlier to expel the closure 100. Once the closure is expelled, the device 20 is held in this position for a short period of time, e.g., 15 to 60 seconds, to allow the foam at the tip of the closure, i.e., the distal end of portion 102, to swell. This action effectively flips the toggle. The insertion device 20 is then removed in a similar manner as described earlier and the closure's filament 104 then retracted, that is, pulled in the direction of arrow 108 in Fig. 8. This action pulls the closure's plug portion 102 back through the puncture or incision 28 in the artery wall until its toggle portion 106 engages the inner surface of the arterial wall to stop further retraction. As the toggle comes into engagement with the arterial wall, it effects the compression of the distal end portion 110 of the plug portion 102. Moreover, the proximal end portion of the plug 102 extends into the puncture or incision in the subcutaneous tissue 22A to a point closely adjacent the skin 22. These actions effectively seal the puncture or incision from the passage of blood therethrough.

It should be noted that the engagement of the toggle with the inner surface of the artery wall can either be direct

r indirect, the latter being through the interposed deformed istal end portion of the plug 102. In either event, the toggle erves to act as a stop precluding the closure 100 from being ulled out of sealing engagement with the puncture or incision 8.

In lieu of the use of the toggle/foam plug closure 100, ne can utilize an alternative closure 200. The closure 200 asically comprises a preformed foam plug having an enlarged istal end portion 106 (See Figs. 11 and 12) serving as the eretofore described holding member, a proximally located od-like portion 102 (See Figs. 11 and 12) serving as the eretofore described sealing member and a retraction filament 04 secured thereto. The closure 200 is preferably formed of a ense collagen foam with long collagen fiber reinforcement so nat it has a high expansion ratio (wet-to-dry) and good echanical wet strength.

The closure 200, like closures 30 and 100 is held ithin the tubular portion 32 of the insertion device 20 in a ompressed state and with its holding portion 106 located mmediately adjacent the outlet 34. For sealing punctures or ncisions in arteries the device 20 is introduced into the :tery in the manner as described heretofore. The pusher member 3 then pushes the foam closure out of the outlet, whereupon the olding portion 106 swells upon contact with the blood in the :tery. The insertion device 20 is then removed so that the losure 200, now swollen, hangs up at the puncture or incision 3 within the arterial wall, i.e., the enlarged holding member ortion 106 engages the inner surface of the arterial wall and ne sealing portion 102 extends fully through the puncture or ncision into the subcutaneous tissue 22A. The retraction of ne filament fully seats the closure in place so that the ealing portion extends fully through the puncture or incision n the artery wall and with its proximal end located within the ubcutaneous tissue closely adjacent the skin.

The advantage of the preformed foam closure as just escribed over the toggle/plug closure 100 is that it is

As mentioned earlier, it is frequently desirable to be ble to seal a puncture or incision in body organs or tissue ther than blood vessels. For example, in cases where ercutaneous transhepatic punctures are made into the gall ladder for purposes of introducing chemicals or mechanical nstruments, there exists a very real risk of bile leakage into he peritoneum via the liver puncture site, thereby resulting in dangerous possibility of peritonitis. The closures 30, 100 nd 200, as described heretofore, can be utilized to seal such ercutaneous punctures or incisions to eliminate the risks of ile leakage. For example, as shown in Fig. 11 an insertion evice 20 with a closure 100 or 200 disposed therein is ntroduced through the puncture or incision 28 in the right lobe f the liver and through the puncture or incision in the gall ladder so that the device's outlet 34 extends just beyond its ntroducer sheath 26. The plunger 38 is then pressed to eject ne closure so that the holding portion 106 thereof is located ithin the gall bladder and in engagement with the inner surface nereof, while the sealing portion 102 extends through the ncture or incision in the gall bladder and into the puncture : incision in the liver. Alternatively, the closure 100/200 ay be left in the incision or puncture 28 in the liver alone, : that makes best sense from a medical/surgical standpoint.

The subject invention is also useful for effecting the aling of percutaneous incisions or punctures in the heart, ich as could result from a wound. In this connection, as shown Fig. 12, a wound penetrating the left lung and left ventricle ay be sealed by introducing the insertion device 20 with a osure 100/200 therein through the wound, through the puncture the lung, and into the puncture in the left ventricle. The osure 100/200 is then ejected so that its holding portion 106 located within the left ventricle, while its sealing portion 2 extends through the puncture in the left ventricle wall and rough the puncture in the left lung. In such applications, it preferred that the closure member 100/200 be configured so at its sealing portion 102 is of a substantial length to

tend not only through the puncture in the left ventricle, but so the puncture in the lung and through the wound in the skin some exterior point closely adjacent the skin. Thus, the osure 100/200 acts as a tamponade.

As should be appreciated by those skilled in the art, e device and methods of this invention as well as the closure vice mentioned in my copending United States Patent plication, can be puncture in any body tissue or organ to event the flow of fluid through that puncture or incision from e body portion to another.

Without further elaboration the foregoing will so fully lustrate my invention that others may, by applying current or ture knowledge, adopt the same for use under various nditions of service.

What is claimed as the invention is

1. A closure device for sealing a puncture or incision ɔrmed percutaneously in tissue separating two internal portions ɛ the body of a living being, characterized in that said device ɔmprises a plug means arranged for placement at a predetermined ɔsition within the body of said being and having a first ɔlding portion adapted to engage portions of the tissue ijacent said puncture or incision to hold said plug means in .ace and a second sealing portion formed of an expandable ıterial which expands automatically in response to the ambient ırroundings when in said predetermined position and extending ırough said first puncture of incision to engage the tissue ɔntiguous therewith to seal said puncture or incision from the .ow of a body fluid therethrough between said two internal ɔrtions.

2. The device of Claim 1 characterized in that said :pandable material is a collagen foam.

3. The device of Claim 1 characterized in that said pandable material is a gelatinous foam.

4. The device of Claim 1 wherein said tissue comprises blood vessel and characterized in that said second sealing rtion extends fully through said puncture or incision in the ll of said blood vessel to a point adjacent the skin of the ing.

5. The device of Claim 4 characterized in that wherein id expandable material is a collagen foam.

6. The device of Claim 4 characterized in that said pandable material is a gelatinous foam.

7. The device of Claim 1 wherein said tissue comprises e gall bladder and characterized in that said second sealing rtion extends fully through said puncture or incision in the ll of said gall bladder and into a cooperating puncture or cision in the liver of said being.

8. The device of Claim 7 characterized in that said ɔandable material is a collagen foam.

9. The device of Claim 7 characterized in that said pandable material is a gelatinous foam.

10. The device of claim 1 wherein said tissue mprises the liver of said being and characterized in that said cond sealing portion extends substantially into said puncture incision in said liver.

11. The device of Claim 10 characterized in that said pandable material is a collagen foam.

12. The device of Claim 10 characterized in that said pandable material is a gelatinous foam.

13. The device of Claim 1 wherein said tissue is the art of said being and characterized in that said second aling portion extends through said incision or puncture in id heart to a point closely adjacent the skin of said being.

14. The device of Claim 13 characterized in that said pandable material is a collagen foam.

15. The device of Claim 13 characterized in that said pandable material is a gelatinous foam.

16. The device of Claim 1 further characterized by traction means.

17. The device of Claim 16 characterized in that said traction means comprises a filament secured to said holding tion.

18. The device of Claim 17 characterized in that said ding portion is in the form of a toggle.

19. The device of Claim 18 characterized in that said ament and said toggle are each formed of a biodegradable erial.

20. The device of Claim 1 wherein said tissue is a g of said being and characterized in that said second sealing tion extends through said incision or puncture into said lung a point closely adjacent the skin of said being.

21. The device of Claim 20 characterized in that said pandable material is a collagen foam.

22. The device of Claim 20 characterized in that said pandable material is a gelatinous foam.

23. The method of sealing a small puncture or incision ɔrmed percutaneously in tissue separating two internal portions ɛ the body of a living being by the use of plug means compris- ıg a first holding portion and a second sealing portion formed ɛ an expandable material which expands automatically in ɛsponse to the ambient surroundings when in the body of said ɛing, characterized in that said method comprises the steps of ıserting said plug means percutaneously into said puncture or ıcision so that said first holding portion engages portions of ıid tissue to hold said plug means in place and with said ɛcond sealing portion extending through said puncture or ıcision expanding automatically to engage the tissue contiguous ıerewith to seal said puncture or incision from the flow of a ɔdy fluid therethrough between said two internal portions.

24. The method of Claim 23 wherein said tissue ɔmprises a blood vessel and characterized in that said step of ıserting the plug means is carried out to position said second ɛaling portion fully through said puncture or incision in the ıll of said blood vessel to a point adjacent the skin of said ɛing.

25. The method of sealing a small puncture or incision ɔrmed percutaneously in the gall bladder by use of a plug means ɔmprising a first holding portion and a second sealing portion ɔrmed of an expandable material, characterized in that said thod comprises the steps of inserting said plug means rcutaneously into said puncture or incision so that said first ldding portion engages portions of said gall bladder to hold id plug means in place and with said second sealing portion tending fully through said puncture or incision in the wall of id gall bladder and into a cooperating puncture or incision in e liver of said being to seal said puncture or incision from e flow of a body fluid therethrough.

26. The method of sealing a small puncture or incision rmed percutaneously in the liver of a living being by the use plug means comprising a first holding portion and a second aling portion formed of an expandable material. characterized that said method comprises the steps of inserting said plug ans percutaneously into said puncture or incision so that said rst holding portion engages portions of said liver to hold id plug means in place and with said second sealing portion tending substantially into said puncture or incision in said ver to engage the tissue contiguous therewith to seal said ncture or incision from the flow of body fluid therethrough.

27. The method of sealing a small puncture or incision rmed percutaneously in the heart of a living being by use of ig means comprising a first holding portion and a second aling portion formed of an expandable material, characterized that said method comprises the steps of inserting said plug ans percutaneously into said puncture or incision so that rst holding portion engages portions of said heart to hold id plug means in place and with said second sealing portion tending through said incision or puncture in said heart to a int closely adjacent the skin of said being and engaging the ssue contiguous therewith to seal said puncture or incision om the flow of body fluid therethrough.

28. The method of sealing a small puncture or incision rmed percutaneously in a lung of a living being by the use of ig means comprising a first holding portion and a second aling portion formed of an expandable material, characterized that said method comprises the steps of inserting said plug ans percutaneously into said puncture or incision so that said rst holding portion engages portions of said lung to hold said ig means in place and with said second sealing portion tending fully through said puncture or incision in said lung a point closely adjacent the skin of said being to engage the ssue contiguous therewith to seal said puncture or incision om the flow of a body fluid therethrough.

29. The method of Claim 25 wherein said second sealing ortion automatically expands in response to the ambient urroundings when in the body of said being in said puncture or ncision.

30. The method of Claim 26 wherein said second sealing ɔrtion automtically expands in response to the ambient ırroundings when in the body of said being in said puncture or ıcision.

31. The method of Claim 27 wherein said seocnd sealing ɔtion automatically expands in response to the ambient ırroundings when in the body of said being in said puncture or ıcision.

32. The method of Claim 28 wherein said second sealing ɔrtion automatically expands in response to the ambient ırroundings when in the body of said being in said puncture or ıcision.

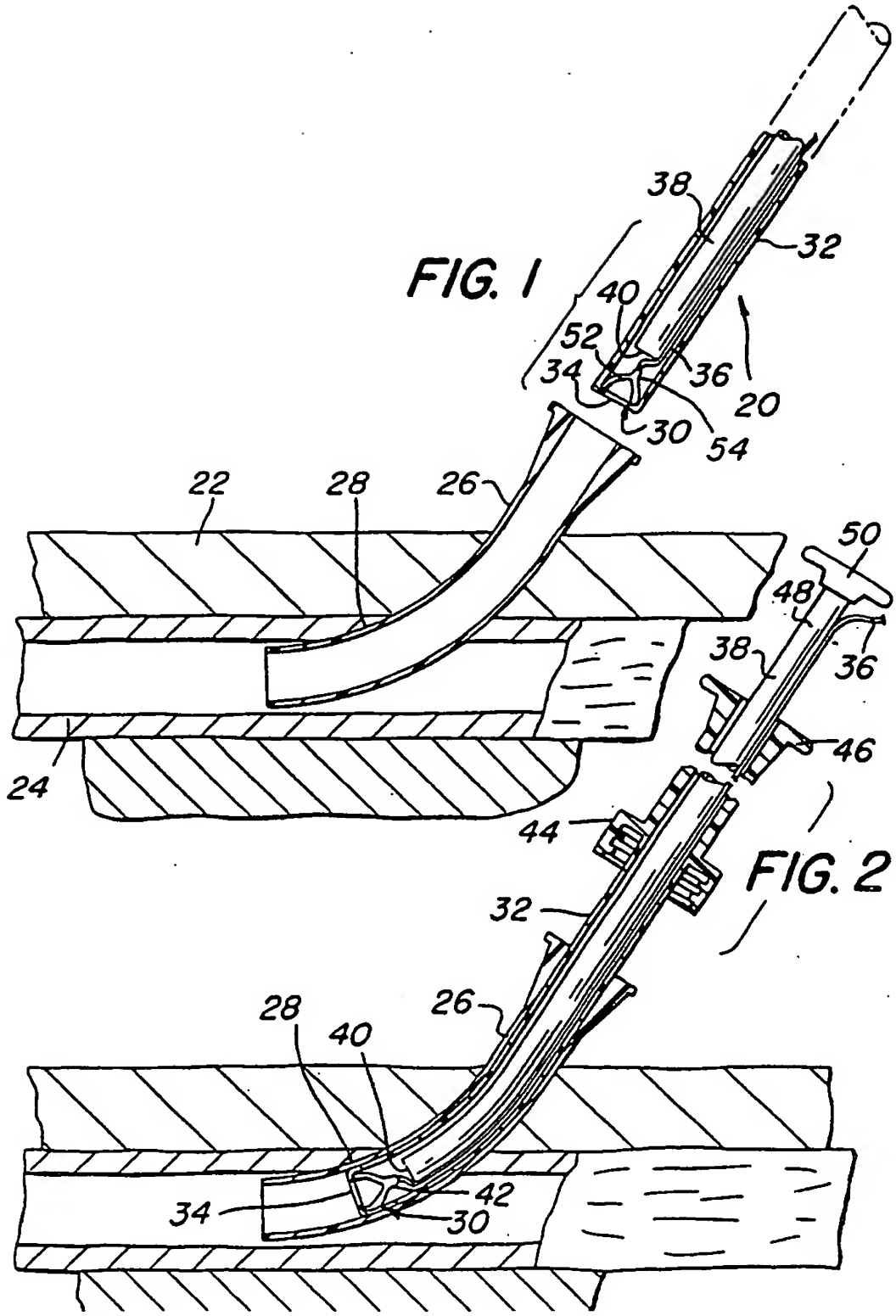
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FIG. 1

FIG. 2

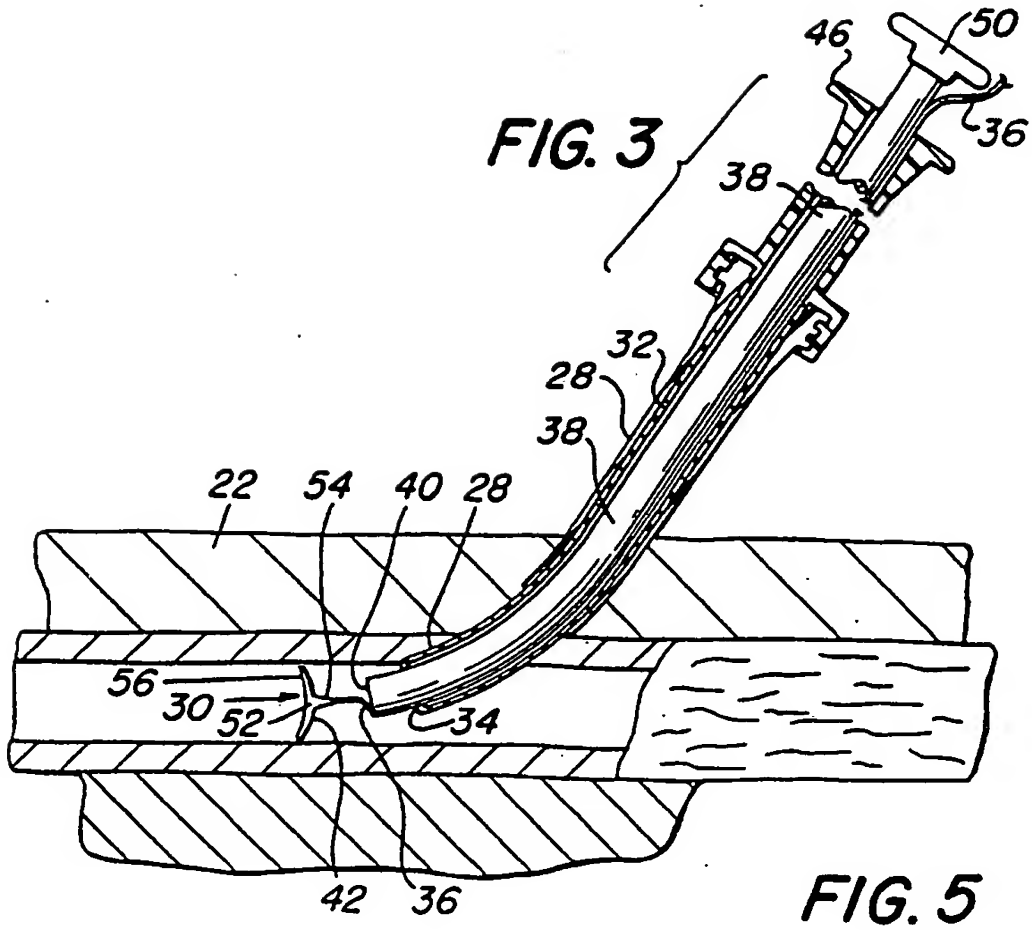
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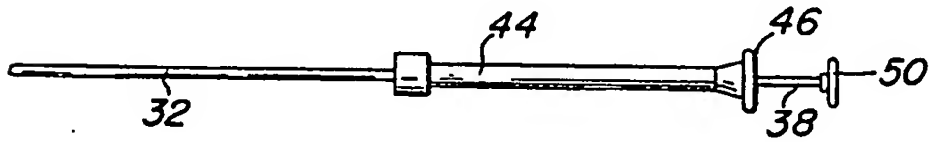
FIG. 5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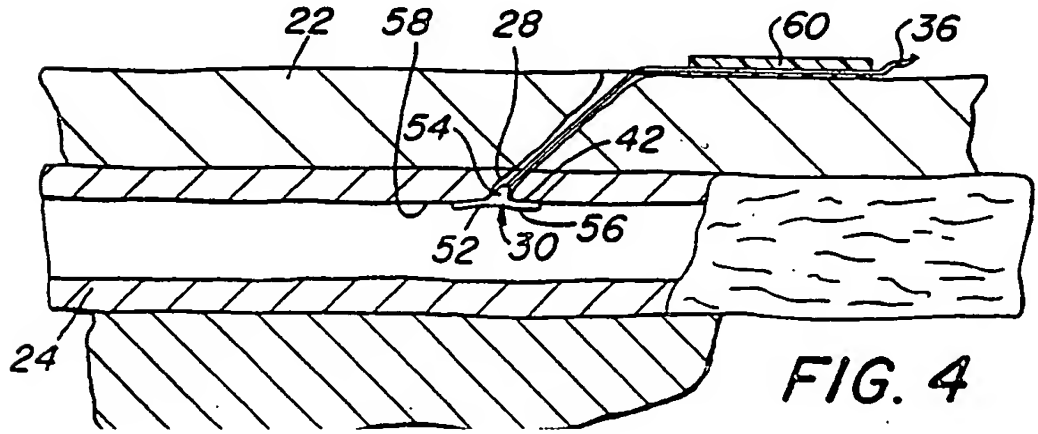
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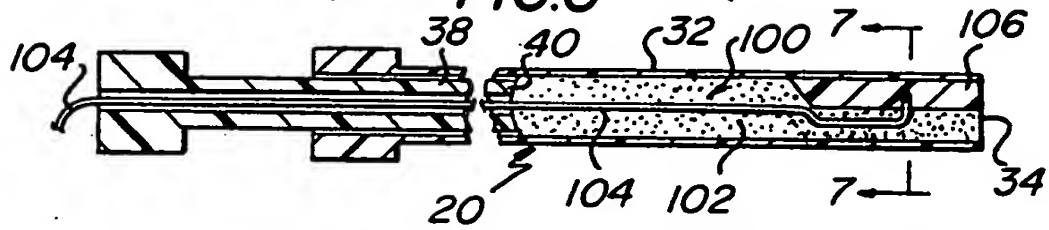
FIG. 4

FIG.6



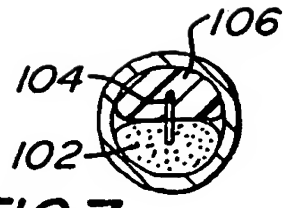


FIG.7

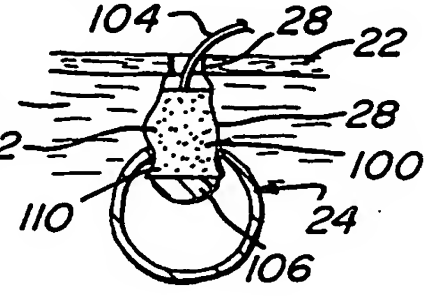


FIG.10

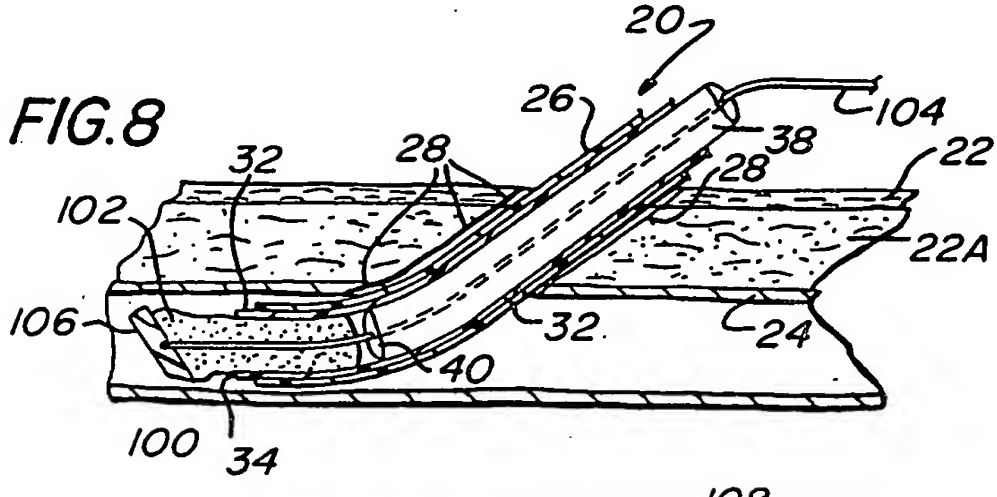


FIG.8

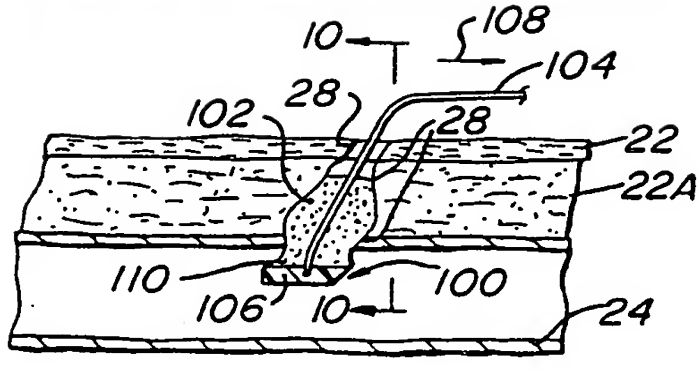


FIG.9

FIG. 11

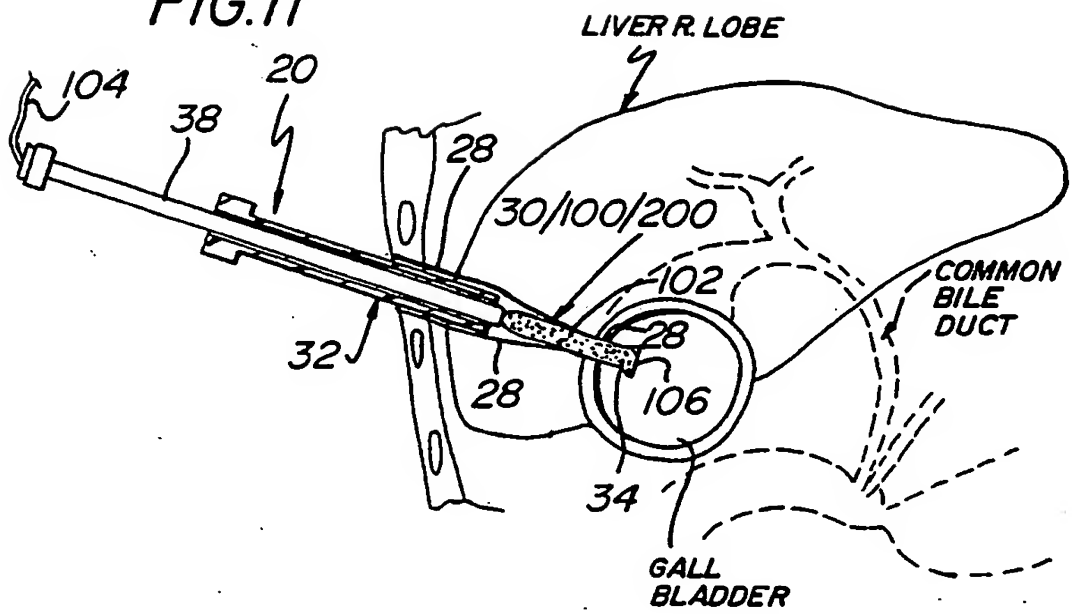
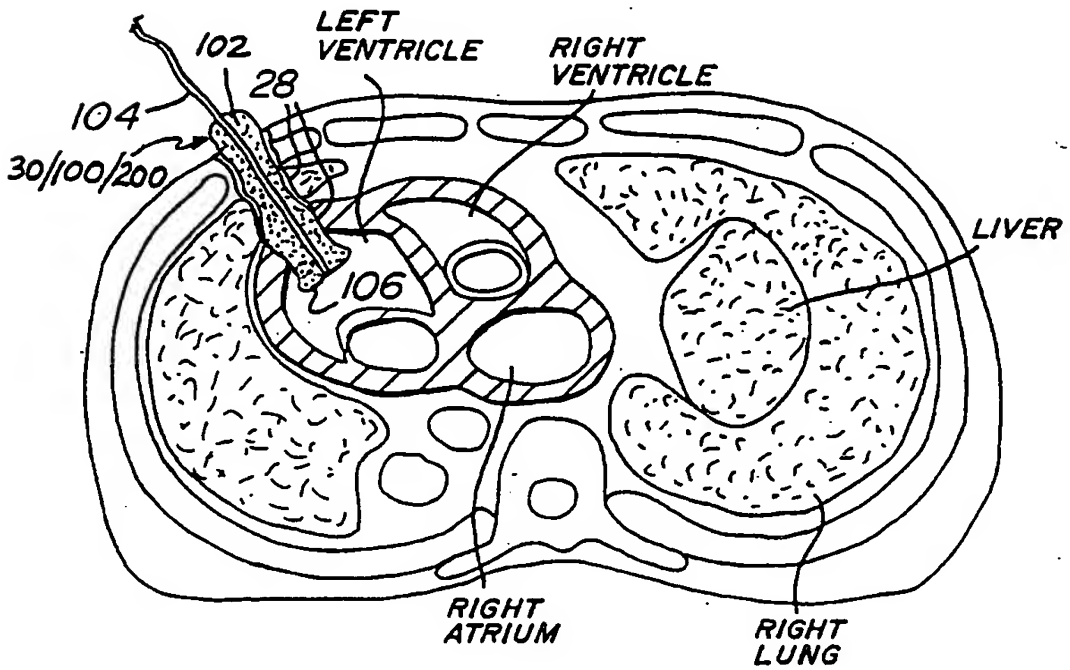

LIVER R. LOBE
104
38
20
28
30/100/200
102
COMMON BILE DUCT
28
32
28
106
34
GALL BLADDER

FIG. 12


LEFT VENTRICLE
RIGHT VENTRICLE
102
28
104
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106
LIVER
RIGHT ATRIUM
RIGHT LUNG

INTERNATIONAL SEARCH REPORT

International Application No PCT/US89/02016

I. CLASSIFICATION OF SUBJECT MATTER (if several classification symbols apply, indicate all) [6]

According to International Patent Classification (IPC) or to both National Classification and IPC

IPC (4) A61M 1/03

U.S. CL. 128/334R

II. FIELDS SEARCHED

Minimum Documentation Searched [7]

Classification System	Classification Symbols
U.S.	128/92YR, 155,325,334R,831,843,865,887,897-899 604/15,60,285,288 600/32,623/1,11

Documentation Searched other than Minimum Documentation to the Extent that such Documents are Included in the Fields Searched [8]

III. DOCUMENTS CONSIDERED TO BE RELEVANT [9]

Category *	Citation of Document, [11] with indication, where appropriate, of the relevant passages [12]	Relevant to Claim No. [13]
A	US,A, 1,794,221 (WASHBURN ET AL) 24 FEBRUARY 1931, See Figures 1-4.	1-22
A	US,A, 3,874,388 (KING ET AL) 01 APRIL 1975, See entire document.	1-24,27,31
A	US,A, 4,007,743 (BLAKE) 15 FEBRUARY 1977, See entire document.	1-24,27,31
A	US,A, 4,154,226 (HENNIG ET AL) 15 MAY 1979, See abstract.	1-22
A	SU,A, 782,814 (VIONOV ET AL), 30 NOVEMBER 1980, See entire document.	1-24,27,31
A	US,A, 4,587,969 (GILLIS) 13 MAY 1986, See abstract.	1-22
A	US,A, 4,650,488 (BAYS ETAL) 17 MARCH 1987.	1-22
P,A	US,A, 4,744,364 (KENSEY) 17 MAY 1988. See abstract.	1-32

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"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"&" document member of the same patent family

IV. CERTIFICATION

Date of the Actual Completion of the International Search	Date of Mailing of this International Search Report
10 July 1989	10 AUG 1989
International Searching Authority	**Signature of Authorized Officer**
ISA/US	Ralph Lewis

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